

6th European Meeting on Visual and Physiological Optics
Dublin, 20-22 August 2012



Estimation of the ocular point spread function by retina modeling

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Point spread function



- ▶ Motivation: improve retinal imaging by taking advantage of the intrinsic properties of the human eye
- ▶ For this, we estimate the point spread function (PSF)
 - ▶ Ocular aberrations can be estimated
 - ▶ Deconvolution methods that reduce the image blurring can be used by knowing the PSF
 - ▶ Blind deconvolution techniques are often biased by the initial guess of the point spread function. PSF estimation gives a better estimate for this initial guess
- ▶ Method is independent of the imaging acquisition technique
- ▶ Based on identification of retinal cells and modeling them

Theory



- ▶ In the case of multi-frame image, made of m frames of the same object :

$$\sum_{j=1}^m i_j(\mathbf{r}) = \sum_{j=1}^m p_j(\mathbf{r}) \otimes o(\mathbf{r}) + n_j(\mathbf{r})$$

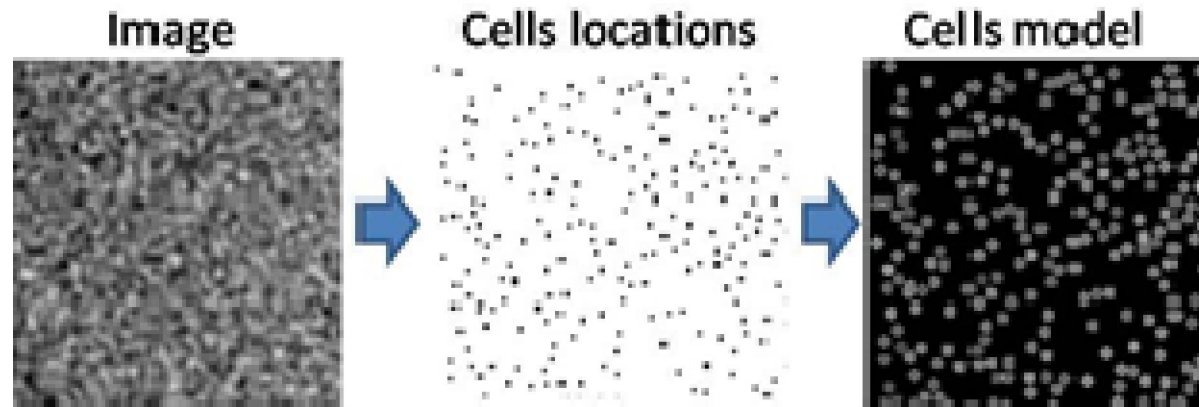
- ▶ We wish to replace the object $o(r)$ with model $c(r)$ of the cells
- ▶ To replace the object $o(r)$ with $c(r)$, we need to introduce a new term, $b(r)$, which compensates for all the other features beside cells

$$\sum_{j=1}^m i_j(\mathbf{r}) - b_j(\mathbf{r}) = \sum_{j=1}^m p_j(\mathbf{r}) \otimes c(\mathbf{r}) + n_j(\mathbf{r})$$

- ▶ For a small retinal area, $b(r)$ is constant (background)
- ▶ In the Fourier domain the PSF is

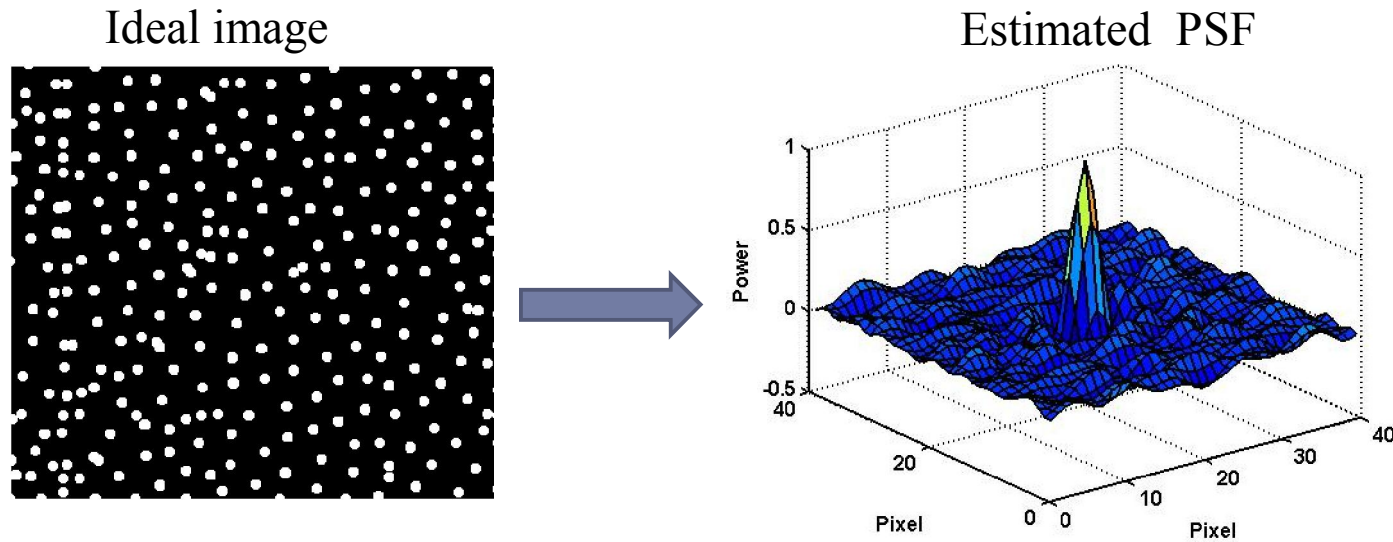
$$\sum_{j=1}^m P_j(\boldsymbol{\omega}) = \frac{\sum_{j=1}^m I_j(\boldsymbol{\omega}) - b_j \delta_j(\boldsymbol{\omega}) - N_j(\boldsymbol{\omega})}{C(\boldsymbol{\omega})}$$

Retinal cells' model - $c(r)$ term

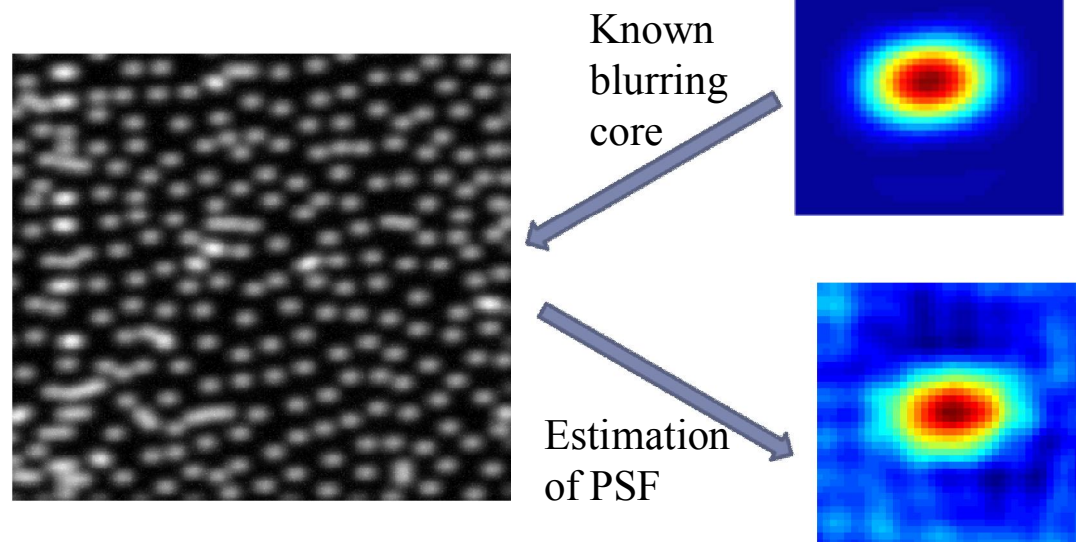


- ▶ Finding the cells' positions in the image, using circular matched filter
- ▶ We replace each cell location with a fixed size circular disc
 - ▶ Discs diameter is determined by the half-height width of their averaged radial intensity profile
- ▶ We determine each disc intensity by the average intensity of the cell in the image
- ▶ Assumptions:
 - ▶ Rods cells are below the resolution limit, therefore ignored
 - ▶ Cones have approximately the same size in the image

Checking the method – synthetic image



Blurring image using blurring core and noise

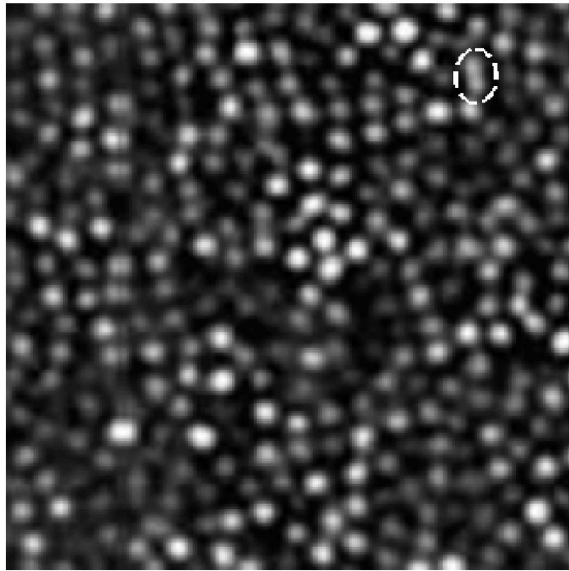


Results – adaptive optics image

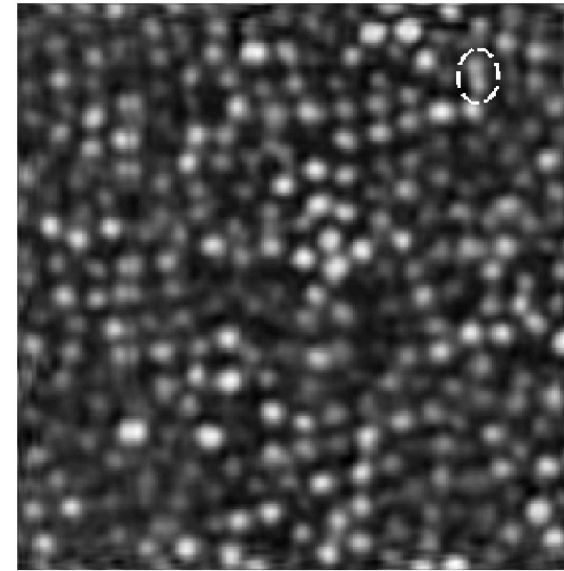


- ▶ Adaptive optics image, taken by retinal camera (courtesy of Dr. Laurent Vabre, Imagine Eyes).

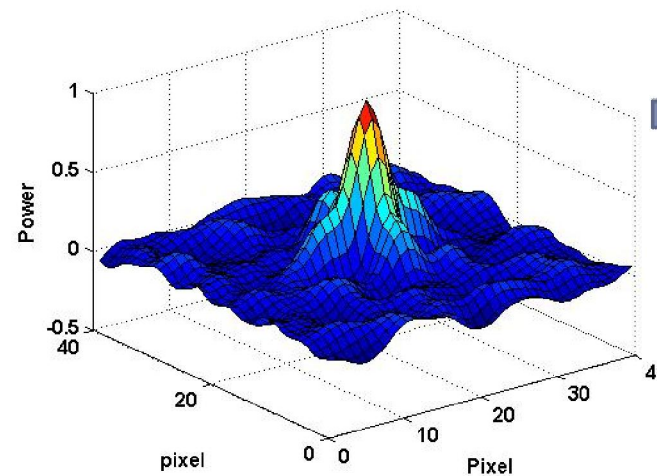
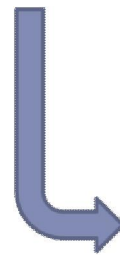
Image



Reconstructed image



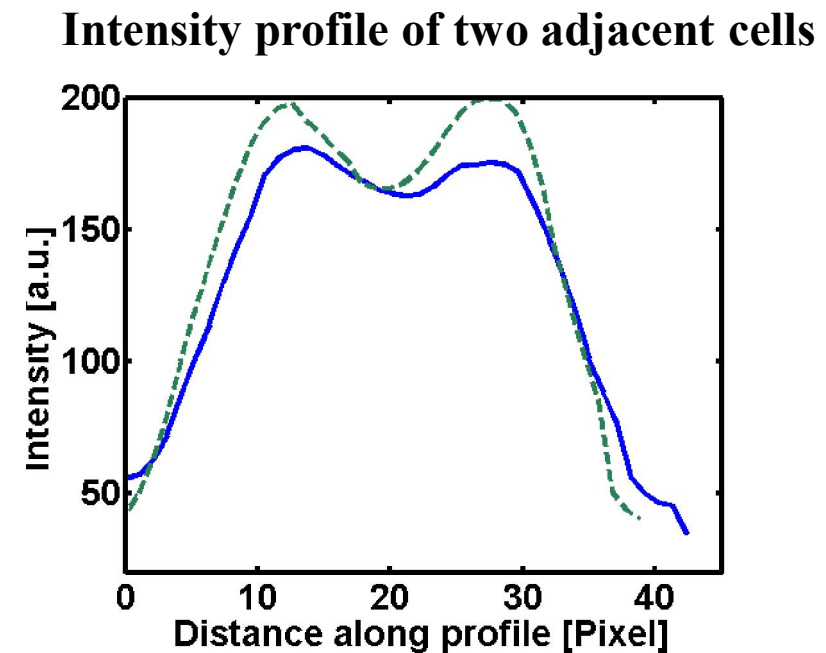
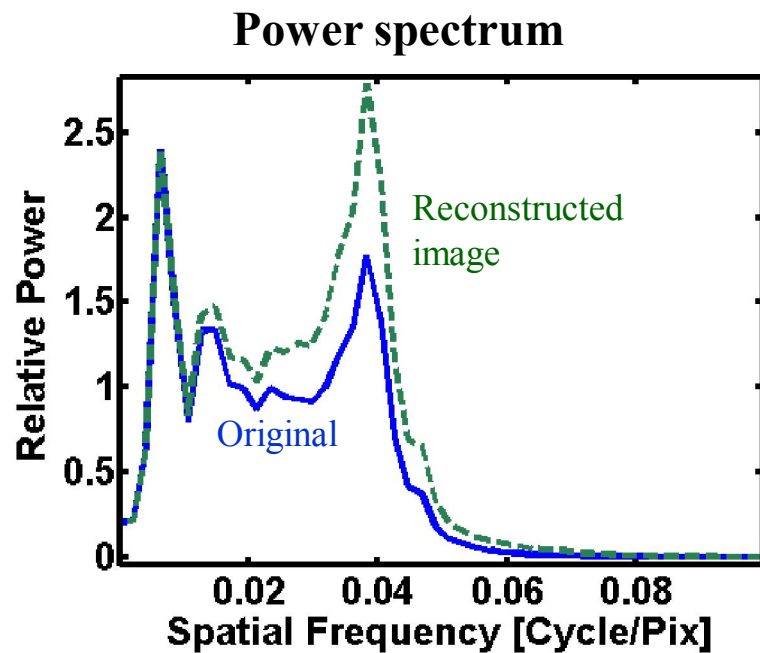
PSF estimation



Reconstruction:
Wiener filter



Results – adaptive optics image analyze

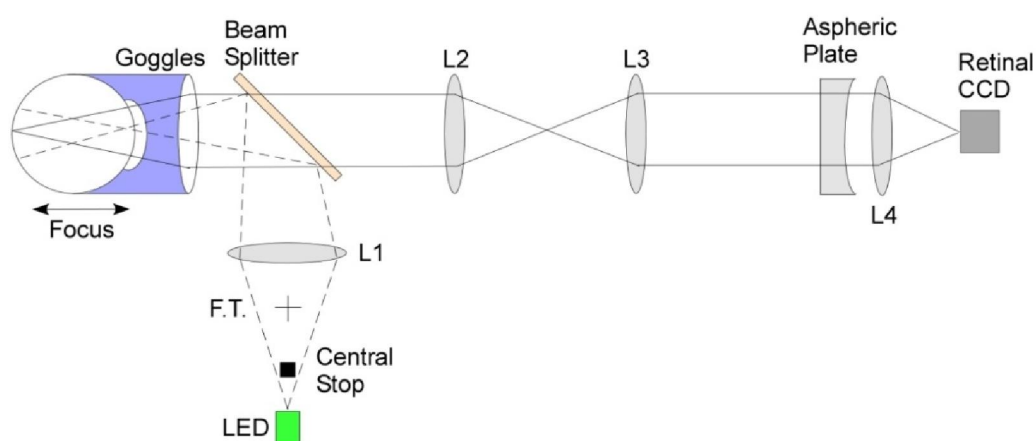


- ▶ Biggest improvement in the power spectrum corresponds to the spatial frequency of minimal inter-cell distances
- ▶ Intensity profile of two adjacent cells (almost unresolved) shows local improvement in contrast

Other retinal imaging methods



- ▶ We implement the PSF estimation method on other imaging methods



- ▶ Immersion method:

- ▶ Corneal immersion by saline solution, to reduce the optical power of the cornea and replacing it by off-the-shelf lens.
- ▶ Reduction of the remaining spherical aberration by aspheric plate

- ▶ Direct method:

- ▶ Similar to the immersion method but without immersion goggle and aspheric plate

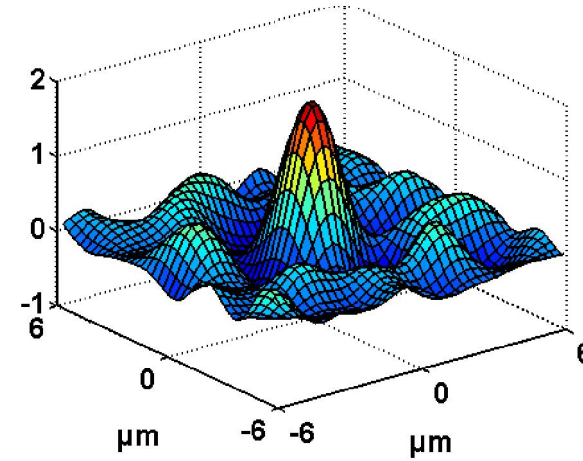
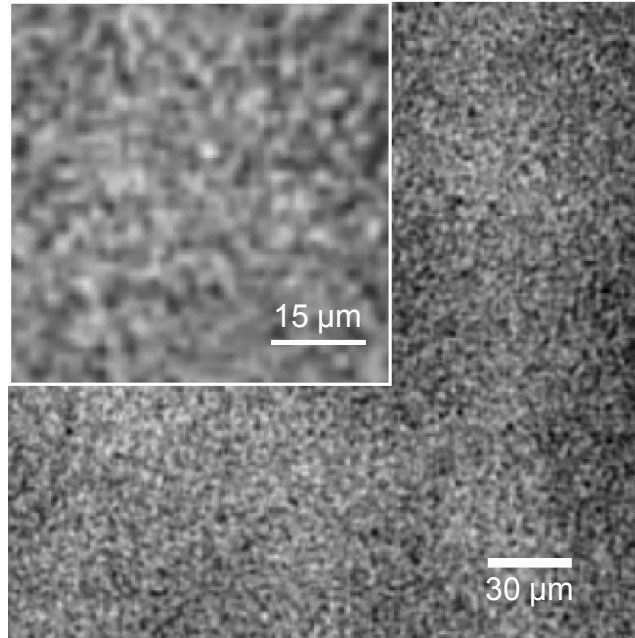
- ▶ We enhance the resolution of both methods by registration of large number of frames.

- ▶ This allows multiple oversampling and dynamic aberrations averaging

Direct imaging results

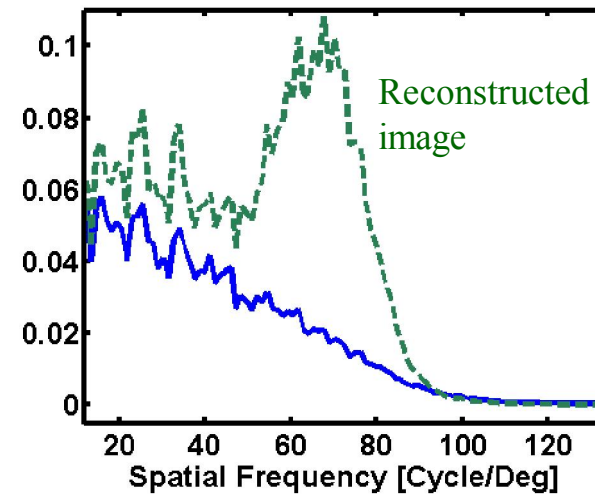
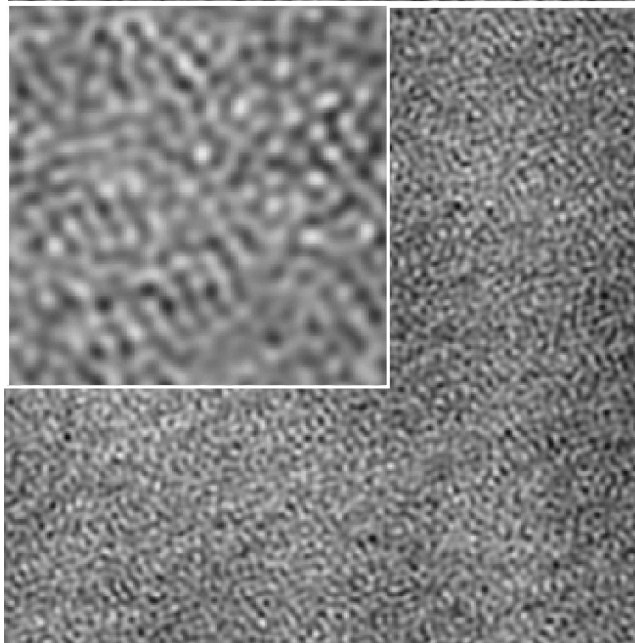


Image



PSF estimation

Wiener reconstruction

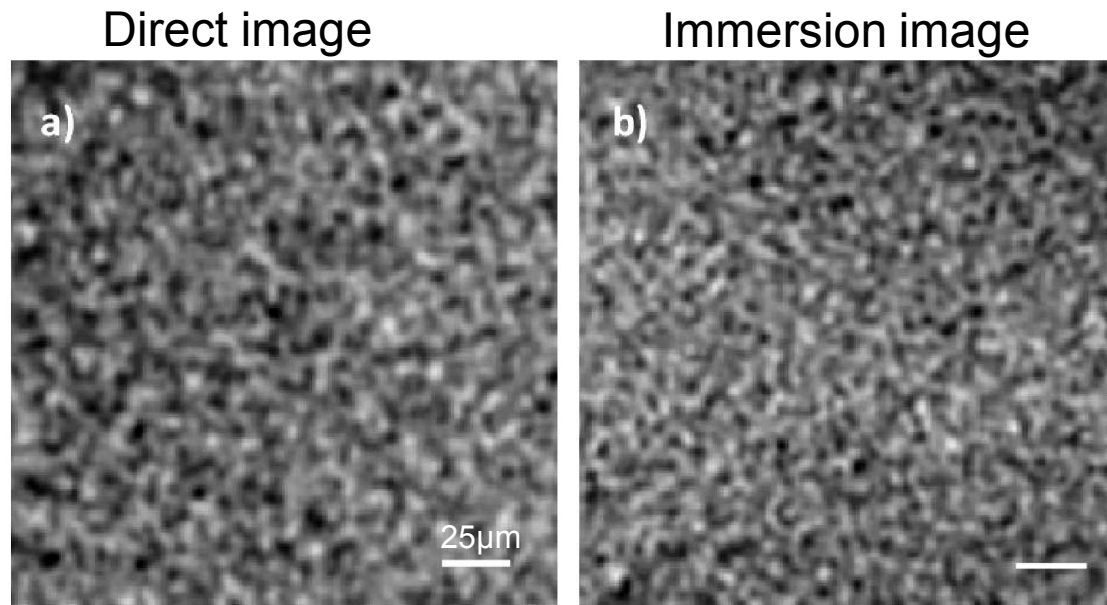


Power spectrum

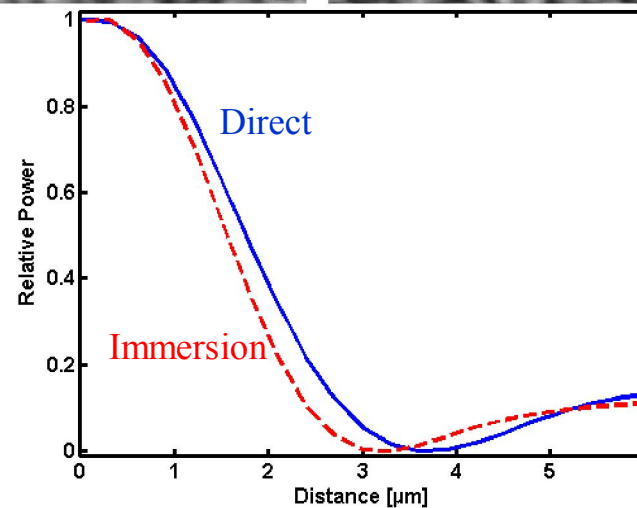
PSF estimation for resolution enhancement analysis



- ▶ The PSF profile demonstrates the better resolution of immersion, compared to direct imaging.



Radial profile of the PSF



Summary



- ▶ We present a method to estimate point spread function by taking advantage of the rather simple geometry of retinal cells
- ▶ In the absence of measured PSF this method can be used to enhance the visibility of cells by deconvolution methods
- ▶ Since the method is based on identification of cells, the estimation is expected to be better when using more resolved images as an input

Reference: N. Meitav and E. N. Ribak, *Optics Letters* 37, 1466-8 (2012).



Thank you for your attention

- ▶ Thanks to
 - ▶ Supervisor : Erez N. Ribak
 - ▶ Lab Collaborators: Eyal Shwartz, Amichai M. Labin
 - ▶ Dr. Alexander Goncharov - Applied Optics Group, NUI Galway
 - ▶ Dr. Laurent Vabre, Imagine Eyes Ltd., France